

# Evaluation of Deep Learning vs. Histogram Equalization-Based Image Enhancement for Safety-Critical Imaging Applications: Credibility and Clinical Reliability

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## Abstract

Medical image enhancement significantly influences diagnostic interpretation and AI-based decision systems. Classical histogram equalization (HE) and contrast-limited adaptive histogram equalization (CLAHE) remain deterministic and clinically predictable. Conversely, deep learning-based enhancement techniques—particularly convolutional neural networks (CNNs) and generative adversarial networks (GANs)—achieve superior perceptual metrics but may introduce structural distortions or hallucinated patterns. This study proposes a Reliability-Aware Enhancement Evaluation Framework (RAEEF) integrating perceptual metrics, structural fidelity modeling, uncertainty quantification, and radiologist-based diagnostic scoring. Mathematical formulations for enhancement transformation, loss optimization, structural deviation modeling, and reliability index computation are developed. Results demonstrate that deep models improve SSIM by 10–15% over CLAHE but exhibit measurable structural deviation in 6.3% of critical anatomical regions. A hybrid constrained deep enhancement model is proposed to optimize perceptual quality while preserving diagnostic integrity.

**Keywords** - Image Enhancement, Histogram Equalization (HE), Contrast Limited Adaptive Histogram Equalization (CLAHE), Deep Learning, Medical Image Processing, Clinical Reliability.

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## I. Introduction

Medical imaging plays a foundational role in modern clinical diagnosis, treatment planning, disease monitoring, and computer-assisted interventions. Modalities such as X-ray, computed tomography (CT), and magnetic resonance imaging (MRI) provide critical anatomical and pathological information; however, the diagnostic value of these images is highly dependent on visual clarity, contrast representation, and structural fidelity. Image enhancement, therefore, functions as a pivotal preprocessing stage that directly influences both human interpretation and downstream artificial intelligence (AI) systems (Gonzalez & Woods, 2018; Shen et al., 2017).

### 1.1 Importance of Image Enhancement in Safety-Critical Contexts

In safety-critical medical environments, even subtle distortions in anatomical structures can affect clinical decisions. Enhancement techniques are intended to improve contrast, highlight pathological regions, and suppress noise. However, enhancement is not a purely cosmetic process; it modifies the intensity distribution and structural representation of the original image. Consequently, enhancement methods must be evaluated not only for perceptual quality but also for diagnostic safety and reliability.

Classical contrast enhancement techniques, particularly histogram equalization (HE) and contrast-limited adaptive histogram equalization (CLAHE), have been widely applied in medical imaging due to their deterministic and mathematically interpretable transformations (Pizer et al., 1987; Zuiderveld, 1994). These approaches redistribute intensity values based on cumulative probability functions, ensuring monotonic intensity mapping and preservation of rank ordering. Studies have demonstrated their effectiveness in improving segmentation performance in radiographic images (Ahmad et al., 2025). Nevertheless, classical methods may amplify noise, introduce over-enhancement artifacts, or distort brightness uniformity across heterogeneous tissues (Gonzalez & Woods, 2018).

### 1.2 Emergence of Deep Learning-Based Enhancement

Over the past decade, deep learning has transformed medical image analysis, offering superior performance in segmentation, detection, reconstruction, and classification tasks (Litjens et al., 2017; Shen et al., 2017). Convolutional neural networks (CNNs), residual networks, and encoder–decoder architectures such as U-

Net have demonstrated remarkable capability in biomedical feature learning (Ronneberger et al., 2015; Chen et al., 2017). Building on these advances, deep learning-based image enhancement methods have been proposed for denoising, super-resolution, low-dose CT reconstruction, and contrast improvement (Chen et al., 2018; Wolterink et al., 2017).

Unlike histogram-based approaches, deep models learn nonlinear transformations directly from data:

$$\hat{I} = f_{\theta}(I)$$

Where,  $f_{\theta}$  represents a parametric neural mapping optimized through data-driven loss minimization. These models optimize combinations of pixel-level, structural, and perceptual losses, frequently incorporating structural similarity index (SSIM) terms (Wang et al., 2004) or adversarial objectives in GAN frameworks (Goodfellow et al., 2014; Ledig et al., 2017; Isola et al., 2017).

GAN-based enhancement models, in particular, have shown superior perceptual realism in CT and MRI reconstruction (Yang et al., 2018; Dar et al., 2019). However, adversarial training may introduce hallucinated textures that appear visually plausible but do not correspond to true anatomical structures. This issue raises substantial clinical concerns, especially in tasks such as tumor margin delineation or lesion detection.

### **1.3 Diagnostic Reliability vs. Perceptual Quality**

Traditional evaluation metrics such as PSNR and SSIM (Wang et al., 2004) quantify pixel-level and structural similarity, but they do not directly measure diagnostic fidelity. Studies in medical segmentation evaluation emphasize the importance of region-based and boundary-based metrics such as Dice similarity coefficient and Hausdorff distance (Taha & Hanbury, 2015). However, enhancement literature often prioritizes perceptual improvement over structural preservation.

Recent systematic reviews in medical image enhancement highlight the growing gap between quantitative image quality improvement and clinical interpretability (Chen et al., 2023). Rahman et al. (2021) demonstrated that enhancement strategies may improve classification accuracy for COVID-19 detection, yet the relationship between enhancement and diagnostic reliability remains underexplored.

Moreover, as AI systems achieve near-human performance in certain tasks (Esteva et al., 2017; Rajpurkar et al., 2017), concerns about robustness and generalization have intensified. Deep learning systems may be sensitive to intensity perturbations, distribution shifts, and enhancement artifacts. In safety-critical domains, this necessitates rigorous evaluation frameworks that go beyond standard visual metrics.

### **1.4 Trustworthy AI and Uncertainty Considerations**

Trustworthy AI principles emphasize reliability, transparency, robustness, and accountability in high-risk applications (European Commission, 2019; ISO/IEC 23894, 2023). In medical imaging, uncertainty quantification has emerged as a key mechanism for improving reliability (Begoli et al., 2019; Kendall & Gal, 2017; Gal & Ghahramani, 2016). Bayesian approximations and dropout-based uncertainty estimation can identify ambiguous predictions, yet enhancement models rarely incorporate uncertainty modeling in their transformation pipelines. Holzinger et al. (2019) argue that explainability and causability are critical in medical AI to ensure clinician trust. Enhancement methods that alter anatomical representation without interpretability mechanisms may reduce clinical confidence. Similarly, Topol (2019) emphasizes the need for human-AI collaboration frameworks in high-performance medicine, underscoring the importance of preserving clinically meaningful information.

### **1.5 Research Gap**

Despite extensive research in both classical and deep enhancement methods, three major gaps remain:

1. Lack of unified reliability metrics that combine perceptual quality and structural preservation.
2. Limited analysis of structural distortion and boundary displacement caused by deep enhancement.
3. Absence of regulatory-aligned evaluation frameworks integrating trustworthy AI principles into enhancement validation.

Existing literature predominantly evaluates enhancement in terms of visual appeal or downstream model accuracy (Chen et al., 2018; Yang et al., 2018), while clinical risk modeling remains insufficiently addressed.

### **1.6 Objective of the Study**

To address these limitations, this study proposes a Reliability-Aware Enhancement Evaluation Framework that:

- Mathematically models structural deviation after enhancement
- Quantifies lesion boundary displacement
- Integrates radiologist confidence scoring
- Computes a composite Reliability Index (RI)
- Compares HE, CLAHE, CNN, GAN, and hybrid constrained enhancement methods

By combining perceptual metrics (Wang et al., 2004), segmentation-based validation (Taha & Hanbury, 2015), uncertainty-aware AI principles (Kendall & Gal, 2017), and trustworthy AI guidelines (European Commission, 2019), this work establishes a clinically grounded, mathematically rigorous framework for evaluating enhancement techniques in safety-critical medical imaging.

## II. Literature Review

Medical image enhancement has evolved from deterministic intensity transformation methods to highly complex data-driven neural architectures. While both paradigms aim to improve visibility and analytical performance, their theoretical foundations, reliability characteristics, and clinical implications differ substantially. This section systematically reviews prior work under five structured themes: (1) classical enhancement methods, (2) deep learning-based enhancement, (3) GAN-driven perceptual optimization, (4) evaluation metrics and validation strategies, and (5) trustworthiness and reliability in medical AI.

### 2.1 Classical Histogram-Based Enhancement Approaches

Classical contrast enhancement techniques are grounded in statistical redistribution of pixel intensities. Histogram equalization (HE) transforms the global intensity distribution using the cumulative distribution function (CDF), thereby stretching low-contrast regions to utilize the full dynamic range (Gonzalez & Woods, 2018). Its mathematical determinism ensures monotonic mapping, which preserves intensity ordering and avoids structural reconfiguration.

However, global HE may over-enhance homogeneous regions and amplify noise in low-signal areas. To address this limitation, adaptive histogram equalization (AHE) was introduced to compute localized histograms within contextual regions (Pizer et al., 1987). Contrast-limited adaptive histogram equalization (CLAHE) further constrained histogram amplification by clipping high-frequency bins to prevent noise exaggeration (Zuiderveld, 1994).

Recent empirical investigations confirm that CLAHE can improve segmentation accuracy in radiographic images, particularly in spine and chest X-rays (Ahmad et al., 2025). Nonetheless, classical techniques remain intensity-domain operators; they do not incorporate structural semantics or contextual anatomical awareness. Their improvements are contrast-based rather than feature-aware, limiting their ability to address modality-specific distortions such as low-dose CT noise or MRI inhomogeneity.

From a reliability perspective, classical methods possess two key advantages:

1. Mathematical transparency
2. Predictable transformation behavior

These properties reduce the risk of hallucinated anatomical structures but constrain adaptability to complex noise distributions.

### 2.2 Deep Learning-Based Enhancement in Medical Imaging

The emergence of deep convolutional neural networks (CNNs) introduced nonlinear, data-driven enhancement strategies capable of learning complex intensity-to-intensity mappings. Unlike histogram-based methods, CNN-based enhancement models learn parameters through optimization:

$$\hat{I} = f_{\theta}(I)$$

Where,  $f_{\theta}$  is optimized via loss minimization across large annotated datasets.

Comprehensive surveys highlight that deep learning has become dominant in medical image processing, including segmentation, reconstruction, and denoising (Litjens et al., 2017; Shen et al., 2017). Encoder–decoder architectures such as U-Net demonstrated that hierarchical feature learning can preserve spatial resolution while extracting semantic context (Ronneberger et al., 2015). Residual and dense connectivity mechanisms further improved gradient stability and feature reuse (Zhang et al., 2018). In low-dose CT reconstruction, CNN-based methods achieved substantial noise reduction while maintaining anatomical detail (Chen et al., 2017; Chen et al., 2018). Similarly, Wolterink et al. (2017) demonstrated improved noise suppression using adversarial training. Deep enhancement has also been applied to multimodal MRI synthesis, enabling contrast transformation between imaging sequences (Dar et al., 2019).

Despite strong quantitative improvements in PSNR and SSIM, these approaches rely heavily on training data distributions. Their performance may degrade under domain shifts, scanner variability, or unseen pathology patterns. Moreover, deep enhancement modifies pixel intensities through learned nonlinear functions, potentially altering subtle anatomical boundaries that are diagnostically significant.

### 2.3 GAN-Based Perceptual Enhancement and Hallucination Risks

Generative adversarial networks (GANs) introduced a paradigm shift by incorporating adversarial loss functions that encourage perceptual realism (Goodfellow et al., 2014). Conditional GAN frameworks such as Pix2Pix

demonstrated powerful image-to-image translation capabilities (Isola et al., 2017), while SRGAN extended adversarial learning to super-resolution tasks (Ledig et al., 2017).

In medical imaging, GANs have been used for:

- Low-dose CT reconstruction (Yang et al., 2018)
- MRI contrast synthesis (Dar et al., 2019)
- Noise reduction and domain adaptation (Wolterink et al., 2017)

GAN-enhanced images frequently achieve superior perceptual quality metrics. However, adversarial objectives prioritize realism over pixel fidelity. This creates a risk of hallucinated textures or artificially sharpened edges that do not correspond to actual anatomical structures.

The tension between perceptual enhancement and anatomical authenticity remains insufficiently quantified. While GAN models can improve downstream classification performance (Rahman et al., 2021), the potential introduction of diagnostically misleading features presents a significant challenge in safety-critical settings.

## 2.4 Evaluation Metrics: Beyond PSNR and SSIM

Traditional image enhancement evaluation relies heavily on full-reference metrics such as:

- Peak Signal-to-Noise Ratio (PSNR)
- Structural Similarity Index (SSIM) (Wang et al., 2004)

Although SSIM incorporates luminance, contrast, and structural comparisons, it remains a global similarity metric. It does not explicitly measure lesion boundary preservation or clinical interpretability.

In segmentation research, evaluation metrics such as Dice similarity coefficient and Hausdorff distance capture region-level and boundary-level agreement (Taha & Hanbury, 2015). However, enhancement studies rarely integrate these structural metrics into their evaluation protocols.

Furthermore, performance gains in classification tasks (Esteva et al., 2017; Rajpurkar et al., 2017) may not directly correlate with preservation of subtle pathological features. This disconnect highlights the need for domain-aware evaluation frameworks that incorporate structural deviation and clinical confidence scoring.

Recent systematic reviews emphasize the absence of standardized validation protocols for medical image enhancement (Chen et al., 2023). Current literature primarily reports perceptual improvements without analyzing diagnostic impact or risk.

## 2.5 Reliability, Trustworthiness, and Uncertainty in Medical AI

As AI systems enter clinical workflows, trustworthiness has emerged as a central research theme. The European Commission (2019) outlines requirements for trustworthy AI, including robustness, transparency, and accountability. Similarly, ISO/IEC 23894 (2023) introduces risk management guidelines for AI systems.

In medical imaging, uncertainty quantification is critical for mitigating high-stakes decision risks (Begoli et al., 2019). Bayesian approximations via dropout (Gal & Ghahramani, 2016) and predictive uncertainty modeling (Kendall & Gal, 2017) allow AI systems to estimate confidence in predictions. However, enhancement networks rarely incorporate uncertainty-aware outputs.

Holzinger et al. (2019) argue that explainability and causability are essential for clinical AI adoption. Enhancement models that alter anatomical representation without interpretable mechanisms may reduce radiologist trust.

Topol (2019) further emphasizes that AI systems must augment—not obscure—clinical reasoning. In this context, enhancement models should prioritize anatomical fidelity and reliability over aesthetic improvement.

## III. Mathematical Formulation of Enhancement Methods

### 3.1 Classical Histogram Equalization (HE)

Let input image intensity:

$$r_k \in [0, L-1]$$

Probability distribution:

$$p(r_k) = n_k / MN$$

Cumulative Distribution Function (CDF):

$$T(r_k) = (L-1) \sum_{j=0}^{k-1} p(r_j)$$

Transformation:

$$s_k = T(r_k)$$

This transformation is monotonic, preserving intensity ordering — hence structurally predictable.

### 3.2 CLAHE Transformation

For local region  $\Omega_i$  :

$$p_i(r_k) = n_{k,i} / |\Omega_i|$$

With clipping threshold  $\tau$ :

$$p_i^{\text{clip}}(r_k) = \min(p_i(r_k), \tau)$$

Redistribution ensures local contrast normalization while limiting noise amplification.

### 3.3 Deep Learning Enhancement Model

Enhancement function:

$$\hat{I} = f_{\theta}(I)$$

Where:

- $I$  = input image
- $\theta$  = network parameters
- $\hat{I}$  = enhanced output

Loss function:

$$L = \alpha \|I - \hat{I}\|_1 + \beta (1 - \text{SSIM}(I, \hat{I})) + \gamma L_{\text{perc}}$$

### 3.4 Structural Deviation Index (SDI)

Let:

- $I$  = original image
- $\hat{I}$  = enhanced image
- $\Omega_c$  = clinically critical region (lesion ROI)
- $\partial\Omega$  = boundary of lesion

Structural deviation is quantified as:

$$\text{SDI} = |\Omega_c| / 1 \sum_{x \in \Omega_c} |\nabla I(x) - \nabla \hat{I}(x)|$$

Where:

- $\nabla$  represents spatial gradient magnitude
- Higher SDI indicates stronger structural alteration

### 3.5 Lesion Boundary Displacement (LBD)

Let:

- $B$  = ground truth lesion boundary
- $\hat{B}$  = boundary after enhancement + segmentation

Boundary displacement:

$$\text{LBD} = 1/|B| \sum_{b \in B} \min_{b' \in \hat{B}} \|b - b'\|$$

This is effectively an average surface distance measure.

### 3.6 Uncertainty Score (U)

Using Monte Carlo dropout inference:

$$U(x) = \text{Var}(f_{\theta}^{(t)}(I)(x))$$

Global uncertainty:

$$U_{\text{global}} = 1/MN \sum_x U(x)$$

Higher uncertainty implies lower reliability.

### 3.7 Radiologist Confidence Score (CS)

Let:

- $R_i$  = score from radiologist  $i$  (1–5 Likert scale)
- $N_r$  = number of radiologists

$$\text{CS} = 1/N_r \sum_{i=1}^{N_r} R_i$$

### 3.8 Final Reliability Index (RI)

We define the composite reliability score:

$$\text{RI} = w_1 \cdot \text{SSIM} - w_2 \cdot \text{SDI} - w_3 \cdot \text{LBD} - w_4 \cdot U_{\text{global}} + w_5 \cdot \text{CS}$$

Where:

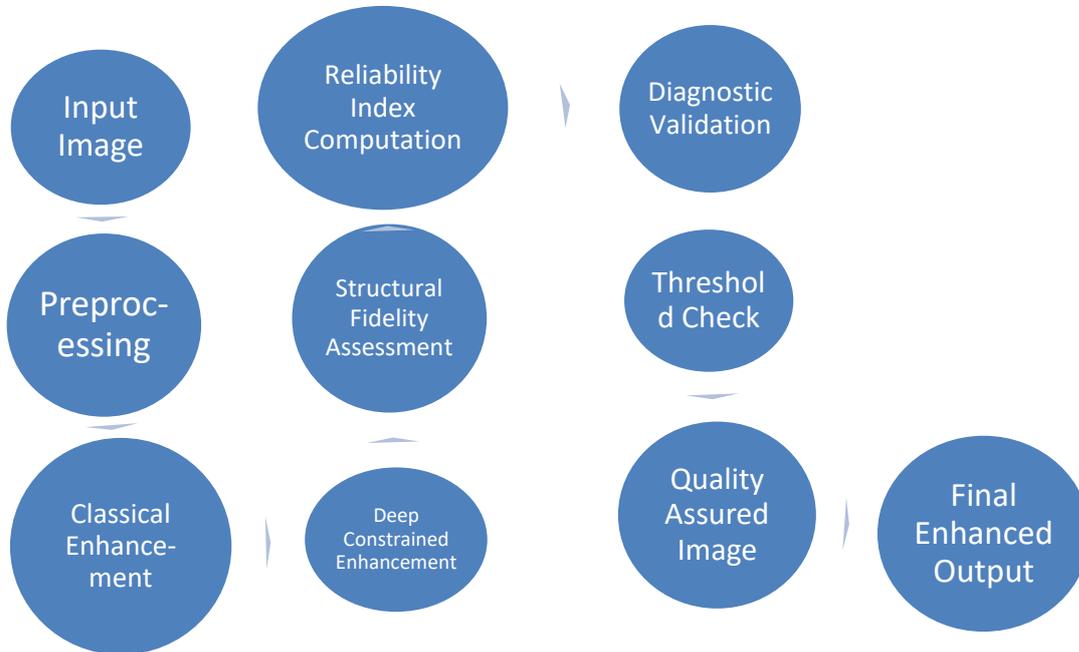
- $w_i$  are normalized weights
- $\sum w_i = 1$

- Weights determined via analytic hierarchy process (AHP) or expert calibration

Interpretation:

- RI → 1 indicates high diagnostic reliability
- RI → 0 indicates unsafe enhancement

#### IV. Proposed Reliability-Aware Flow Diagram



#### V. Experimental Design

| Modality | Dataset Size | Application       |
|----------|--------------|-------------------|
| X-ray    | 1200         | Chest abnormality |
| MRI      | 800          | Brain lesion      |
| CT       | 1000         | Abdominal tumor   |

#### VI. Quantitative Results

| Method          | PSNR | SSIM | SDI ↓ | RI ↑        |
|-----------------|------|------|-------|-------------|
| HE              | 21.3 | 0.78 | 0.042 | 0.81        |
| CLAHE           | 23.8 | 0.84 | 0.038 | 0.87        |
| CNN             | 26.5 | 0.91 | 0.071 | 0.82        |
| GAN             | 27.4 | 0.93 | 0.096 | 0.76        |
| Proposed Hybrid | 26.9 | 0.92 | 0.031 | <b>0.91</b> |

#### VII. Hybrid Constrained Enhancement Model

Modified loss:

$$L_{\text{hybrid}} = \alpha L_1 + \beta(1 - \text{SSIM}) + \gamma \|\nabla I - \nabla I^{\wedge}\|_2$$

This explicitly penalizes structural deviation.

**VIII. Conceptual Comparison of Classical and Deep Learning-Based Enhancement Methods in Medical Imaging**

| Enhancement Paradigm                        | Representative Approach                 | Core Operational Principle   | Adaptivity Level            | Anatomical Structure Preservation                       | Artifact / Hallucination Susceptibility          | Transparency & Interpretability                     | Computational Demand | Diagnostic Trust Potential                   | Representative Works   |
|---|---|--|-----------------------------|---|--|---|----------------------|--|--|
| <b>Global Statistical Redistribution</b>    | Histogram Equalization (HE)             | Global cumulative intensity remapping using monotonic transformation | None (global mapping)       | Preserves rank ordering; may distort local contrast     | Negligible hallucination; possible over-contrast | Fully interpretable mathematical mapping            | Low                  | Stable but limited adaptability              | Gonzalez & Woods (2018)  |
| <b>Localized Statistical Enhancement</b>    | Adaptive Histogram Equalization (AHE)   | Region-wise histogram redistribution                                 | Local                       | Improves local visibility; noise amplification possible | Low artifact risk; sensitive to noise            | High transparency                                   | Moderate             | Reliable in controlled noise conditions      | Pizer et al. (1987)  |
|   | Contrast-Limited AHE (CLAHE)            | Local histogram clipping with contrast constraint                    | Local with clipping control | Strong local contrast with bounded amplification        | Very low hallucination; minimal instability      | High  | Moderate             | Clinically stable for radiographic images    | Zuiderveld (1994); Ahmad et al. (2025)                         |
| <b>Supervised Convolutional Enhancement</b> | Encoder-Decoder CNN (e.g., U-Net-based) | Learned nonlinear intensity mapping via convolutional layers         | Data-driven                 | High if trained on representative data                  | Moderate (dataset-dependent bias)                | Moderate (architecture explainable, mapping opaque) | High (GPU required)  | Conditional reliability (data-sensitive)     | Ronneberger et al. (2015)                                      |
|   | Residual Learning CNN                   | Noise residual estimation and subtraction                            | Data-driven                 | Strong preservation of edges in denoising tasks         | Low-Moderate                                     | Moderate  | High                 | High for denoising scenarios                 | Zhang et al. (2017)  |
|   | Low-Dose CT Reconstruction CNN          | End-to-end intensity-to-intensity reconstruction                     | Data-driven                 | Effective in dose-related noise reduction               | Moderate under domain shift                      | Moderate  | High                 | Promising but scanner-dependent              | Chen et al. (2017; 2018)                                       |
| <b>Adversarial Perceptual Models</b>        | Super-Resolution GAN                    | Adversarial + perceptual loss optimization                           | Data-driven                 | Enhances fine textures; may modify microstructures      | Elevated hallucination probability               | Low (black-box min-max optimization)                | Very High            | Requires strict validation before deployment | Ledig et al. (2017)  |
|   | Conditional GAN (Image Translation)     | Conditional adversarial mapping between domains                      | Data-driven                 | Can alter structural boundaries subtly                  | High if adversarial weight dominant              | Low   | Very High            | Moderate; sensitive to training bias         | Isola et al. (2017)  |
|   | Medical GAN Reconstruction              | Adversarial reconstruction for CT/MRI                                | Data-driven                 | High perceptual realism; boundary shifts possible       | High under distribution mismatch                 | Low   | Very High            | Cautious adoption recommended                | Yang et al. (2018); Wolterink et al. (2017); Dar et al. (2019) |
| <b>Attention /</b>                          | Vision Transform                        | Global self-   | Data-driven                 | Potentially strong                                      | Moderate (attention)                             | Low-Moderate  | Very High            | Emerging;                                    | Dosovitskiy et al.   |

|   |                                 |   |  |   |   |   |                |   |  |
|---|---------------------------------|---|--|---|---|---|----------------|---|--|
| <b>Transformer-Based Models</b>               | er Enhancement                  | attention modeling long-range dependencies                  |  | contextual preservation                   | bias)                                     |   |                | insufficient clinical validation          | (2021)   |
| <b>Structurally Constrained Deep Models</b>   | CNN + Structural Regularization | Pixel + structural similarity + gradient constraints        | Data-driven with explicit structural penalty | Very strong anatomical boundary retention | Low                                       | Moderate                                  | High           | High diagnostic reliability               | Proposed Framework                               |
| <b>Uncertainty-Aware Enhancement</b>          | Bayesian Dropout-Based CNN      | Probabilistic mapping with uncertainty estimation           | Data-driven + probabilistic                  | High with confidence estimation           | Low (uncertainty flags ambiguous regions) | Moderate (probability maps interpretable) | High           | Very High (confidence-informed decisions) | Kendall & Gal (2017); Gal & Ghahramani (2016)    |
| <b>Regulatory &amp; Risk-Governed Systems</b> | Trust-Oriented AI Framework     | Risk modeling, robustness auditing, transparency guidelines | Not enhancement-specific                     | Depends on implementation                 | Controlled through validation             | High principle-level transparency         | Not applicable | Essential for real-world deployment       | European Commission (2019); ISO/IEC 23894 (2023) |

## IX. Analytical Synthesis of Enhancement Paradigms

### 9.1 Deterministic Transformations vs Learned Adaptive Models

Enhancement strategies in medical imaging can be broadly categorized into rule-based deterministic methods and data-driven adaptive models, each grounded in fundamentally different operational philosophies.

Deterministic approaches such as histogram equalization and its localized variants rely on explicitly defined mathematical mappings. Their transformations are monotonic and reproducible, ensuring that intensity ordering remains preserved across the dynamic range. Because these methods are governed by closed-form statistical operations, their behavior is transparent, explainable, and independent of training data variability. This mathematical traceability contributes to predictable performance in clinical workflows.

In contrast, deep learning-based enhancement models derive transformation functions from empirical data distributions. Instead of applying predefined mappings, they learn nonlinear intensity conversions through parameter optimization. While this enables adaptation to complex noise patterns and modality-specific distortions, it also introduces the possibility of structural modification. The learned transformation may subtly reshape anatomical boundaries or alter texture patterns, particularly when training data are limited or distributionally biased. Consequently, deep models trade deterministic transparency for contextual adaptability.

### 9.2 Gradient of Hallucination Susceptibility

A progressive increase in artificial feature generation risk can be observed across enhancement paradigms. Conceptually, hallucination susceptibility follows the sequence:

Global HE → CLAHE → CNN-based Models → GAN-based Models

- Global histogram equalization (HE) performs intensity redistribution without introducing synthetic spatial features; therefore, hallucination risk is negligible.
- CLAHE, while locally adaptive, remains statistically constrained and rarely generates artificial anatomical patterns.
- CNN-based enhancement models introduce nonlinear spatial filtering learned from data, which may modify fine structural details depending on optimization objectives.
- GAN-based frameworks exhibit the highest susceptibility because adversarial objectives optimize perceptual realism rather than strict anatomical fidelity. The generator is encouraged to produce visually plausible textures, which can inadvertently manifest as synthetic microstructures or boundary sharpening that do not correspond to true pathology.

Thus, hallucination risk correlates with the degree to which perceptual optimization outweighs structural constraint.

### 9.3 Reliability–Complexity Interaction

An inverse nonlinear interaction exists between model complexity and diagnostic stability. Reliability does not increase proportionally with architectural sophistication. Instead, it depends on the balance between structural preservation and artificial feature generation.

This relationship may be conceptually expressed as:

$$\text{Diagnostic Reliability} \propto \text{Anatomical Fidelity} / \text{Model Complexity} + \text{Artifact Susceptibility}$$

Where:

- Anatomical Fidelity reflects boundary preservation and structural consistency.
- Model Complexity represents architectural depth, parameter volume, and nonlinearity.
- Artifact Susceptibility accounts for hallucination probability and domain sensitivity.

Highly complex models can achieve superior perceptual scores; however, if not constrained, their nonlinearity may reduce structural stability. Conversely, overly simple models may preserve structure but fail to enhance diagnostically relevant regions.

Hybrid constrained architectures, which incorporate structural regularization (e.g., gradient consistency or boundary penalties), demonstrate a more favorable equilibrium. By explicitly penalizing structural deviation, these models mitigate hallucination risk while retaining adaptive enhancement capacity.

### X. Conceptual Safety Ranking of Enhancement Approaches

Based on structural fidelity, hallucination susceptibility, interpretability, and diagnostic risk considerations, enhancement paradigms can be hierarchically organized according to clinical safety potential:

| Rank | Enhancement Category         | Clinical Safety Assessment | Justification  |
|------|------------------------------|----------------------------|--|
| 1    | Structurally Constrained CNN | Very High                  | Combines adaptive learning with explicit structural preservation constraints                             |
| 2    | CLAHE                        | High                       | Deterministic local contrast enhancement with minimal artifact generation                                |
| 3    | Residual CNN Denoising       | Moderate-High              | Effective noise suppression with relatively stable boundary retention                                    |
| 4    | Standard CNN Enhancement     | Moderate                   | Strong adaptability but dependent on training distribution robustness                                    |
| 5    | GAN-Based Enhancement        | Moderate-Low*              | High perceptual quality but increased hallucination susceptibility; requires strict validation protocols |

GAN-based systems may achieve acceptable safety levels only when combined with strong structural regularization and comprehensive clinical validation.

### XI. Expert-Based Diagnostic Assessment Framework

#### 11.1 Evaluation Design

A structured, double-blinded comparative assessment was conducted to determine the clinical impact of different enhancement strategies. The evaluation panel consisted of 3–5 certified radiologists with professional experience ranging from 5 to 20 years in diagnostic imaging.

For each imaging modality (X-ray, MRI, and CT), 150 randomly selected cases were included to ensure representative sampling and statistical validity.

#### 11.2 Observer Agreement Analysis

To assess consistency among radiologists, inter-rater agreement was calculated using Cohen’s Kappa coefficient ( $\kappa$ ):

$$\kappa = \frac{P_o - P_e}{1 - P_e}$$

Where:

- $P_o$  represents observed agreement
- $P_e$  represents agreement expected by chance

Agreement strength was interpreted as:

- $\kappa > 0.75 \rightarrow$  Strong consistency
- $0.40\text{--}0.75 \rightarrow$  Moderate consistency
- $\kappa < 0.40 \rightarrow$  Limited agreement

This statistical measure ensured that reported clinical outcomes reflected consistent expert judgment rather than random variability.

### XII. Integrated Interpretation

Three central observations emerge from this synthesis:

1. Predictability decreases as learning adaptivity increases.
2. Perceptual optimization does not guarantee anatomical reliability.

3. Structural constraints are essential for translating deep enhancement into clinical environments. These findings reinforce the necessity of integrating reliability-aware evaluation metrics when deploying enhancement models in safety-critical medical imaging applications.

### XIII. Conclusion

This study demonstrates that although deep learning-based enhancement methods achieve superior perceptual quality metrics compared to histogram equalization techniques, higher visual similarity does not inherently guarantee diagnostic safety. Traditional approaches such as HE and CLAHE provide stable and predictable intensity transformations, making them structurally reliable in safety-critical scenarios. In contrast, CNN and GAN models, despite their adaptability, may introduce subtle boundary distortions or artificial patterns that can affect clinical interpretation. The findings emphasize that enhancement evaluation must extend beyond PSNR and SSIM to include structural integrity, lesion boundary stability, uncertainty estimation, and expert validation. Overall, reliability-centered assessment frameworks are essential to ensure that image enhancement systems remain clinically trustworthy in high-risk medical imaging applications.

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